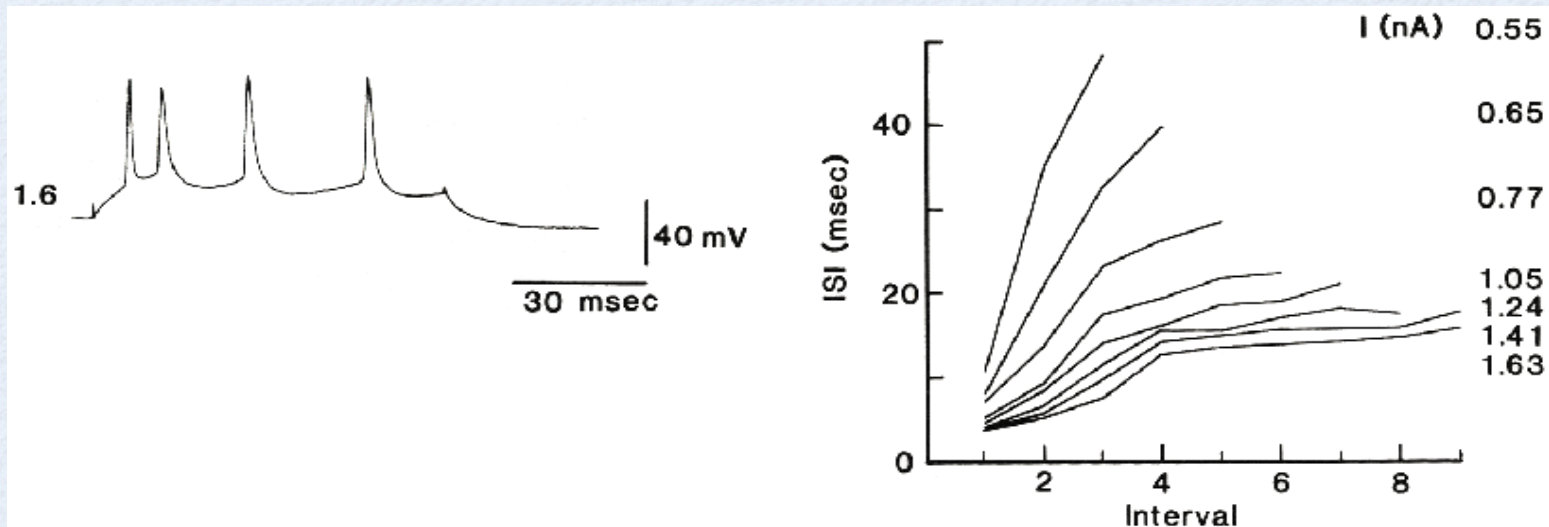


COMPLEX SINGLE CELL MODELS

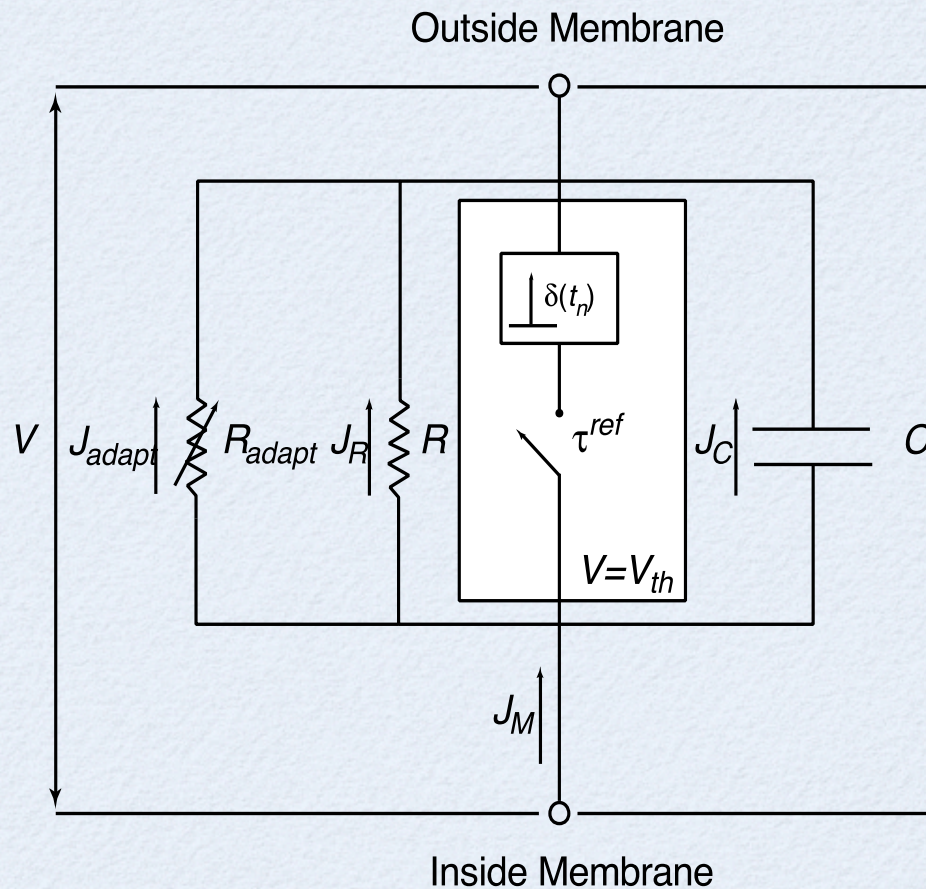
Adaptation

- 'Regular spiking' cells most common in cortex
- Adaptation occurs because of a slow hyperpolarizing K current in these cells



Adapting LIF circuit

- A variable resistor, R_{adapt} , can account for this K

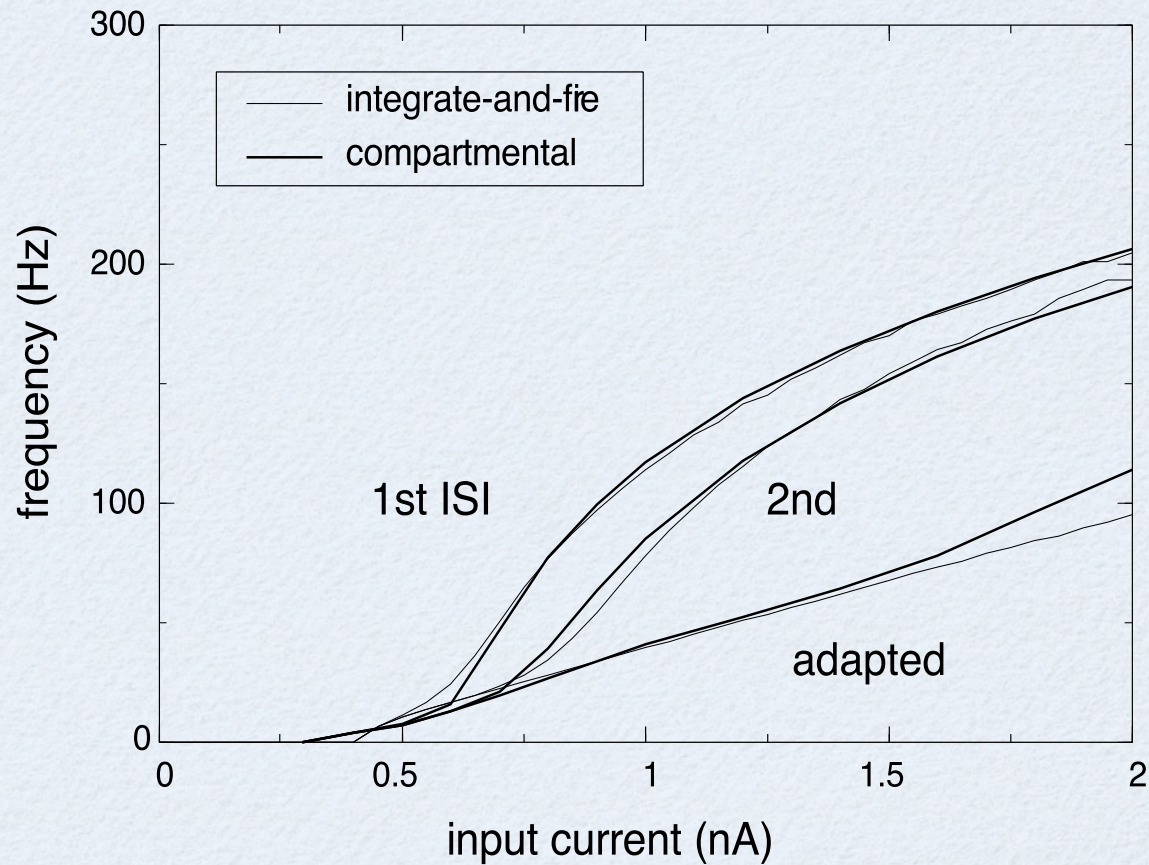


aLIF Behaviour

- Adapt channels stay closed until a spike, then they open (by decreasing R_{adapt}) essentially lowering the reset voltage, making it harder for the next spike to be fired.
- Between spikes, the channels start to close, raising R_{adapt} at a speed determined by τ_{adapt} .

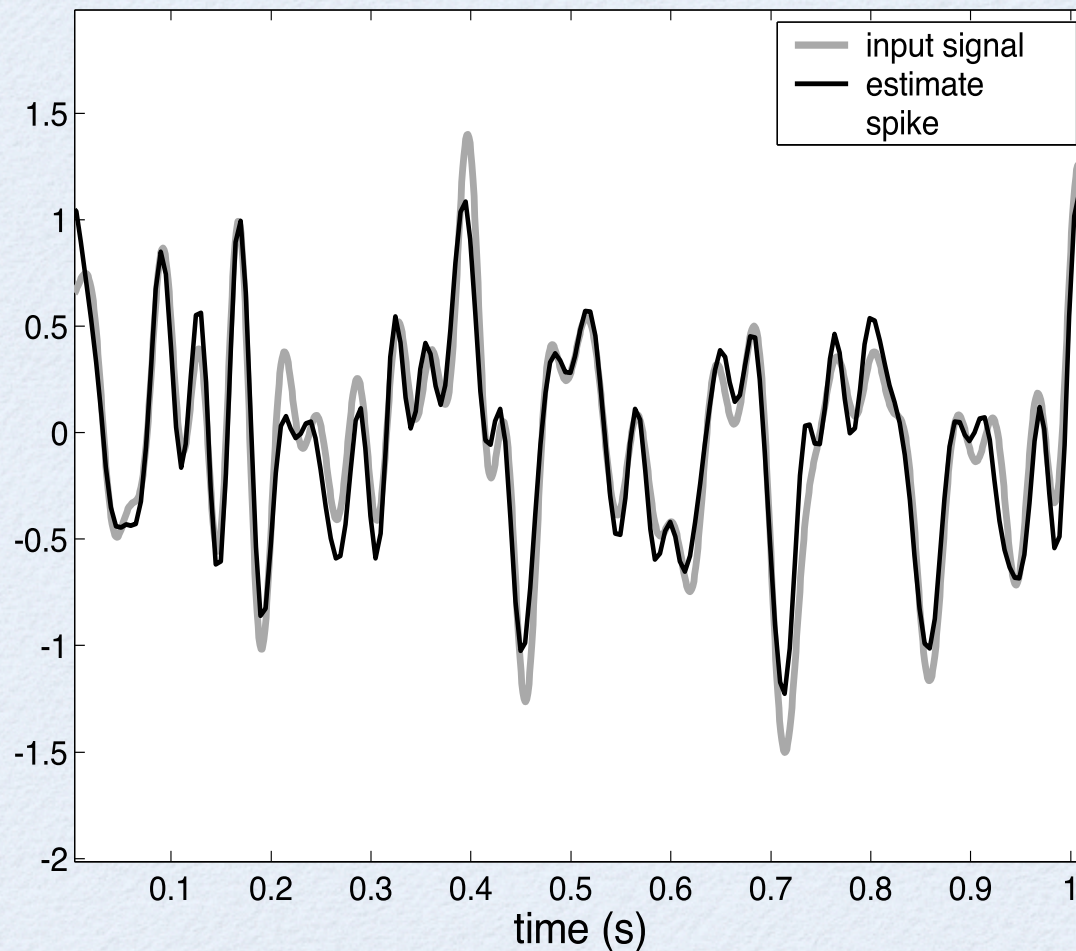
$$\begin{aligned}\frac{dV}{dt} &= -\frac{1}{\tau^{RC}} \left(V \left(1 + \frac{R}{R_{\text{adapt}}} \right) - J_M R \right) \\ \frac{dR_{\text{adapt}}}{dt} &= \frac{R_{\text{adapt}}}{\tau_{\text{adapt}}}\end{aligned}$$

- Comparison of aLIF response function to a complex conductance model



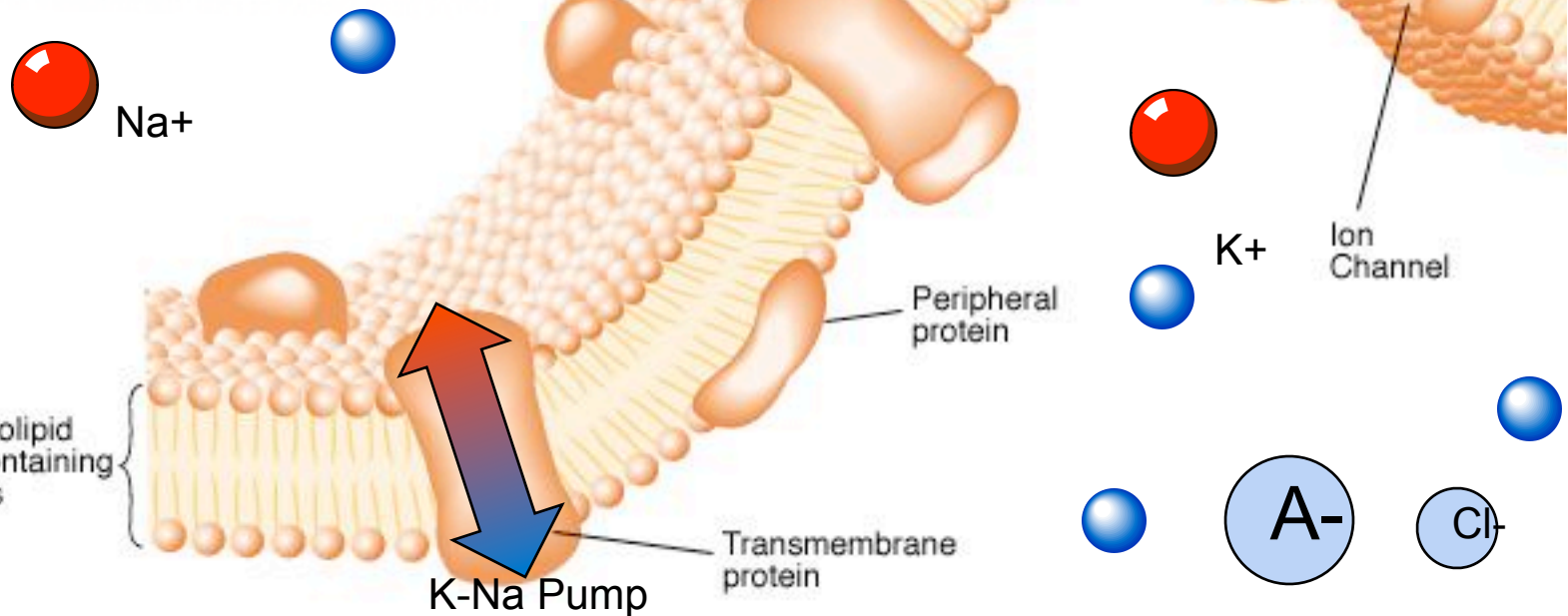
aLIF decoding

- aLIF (as we will see) is more efficient



Ion flow: rest

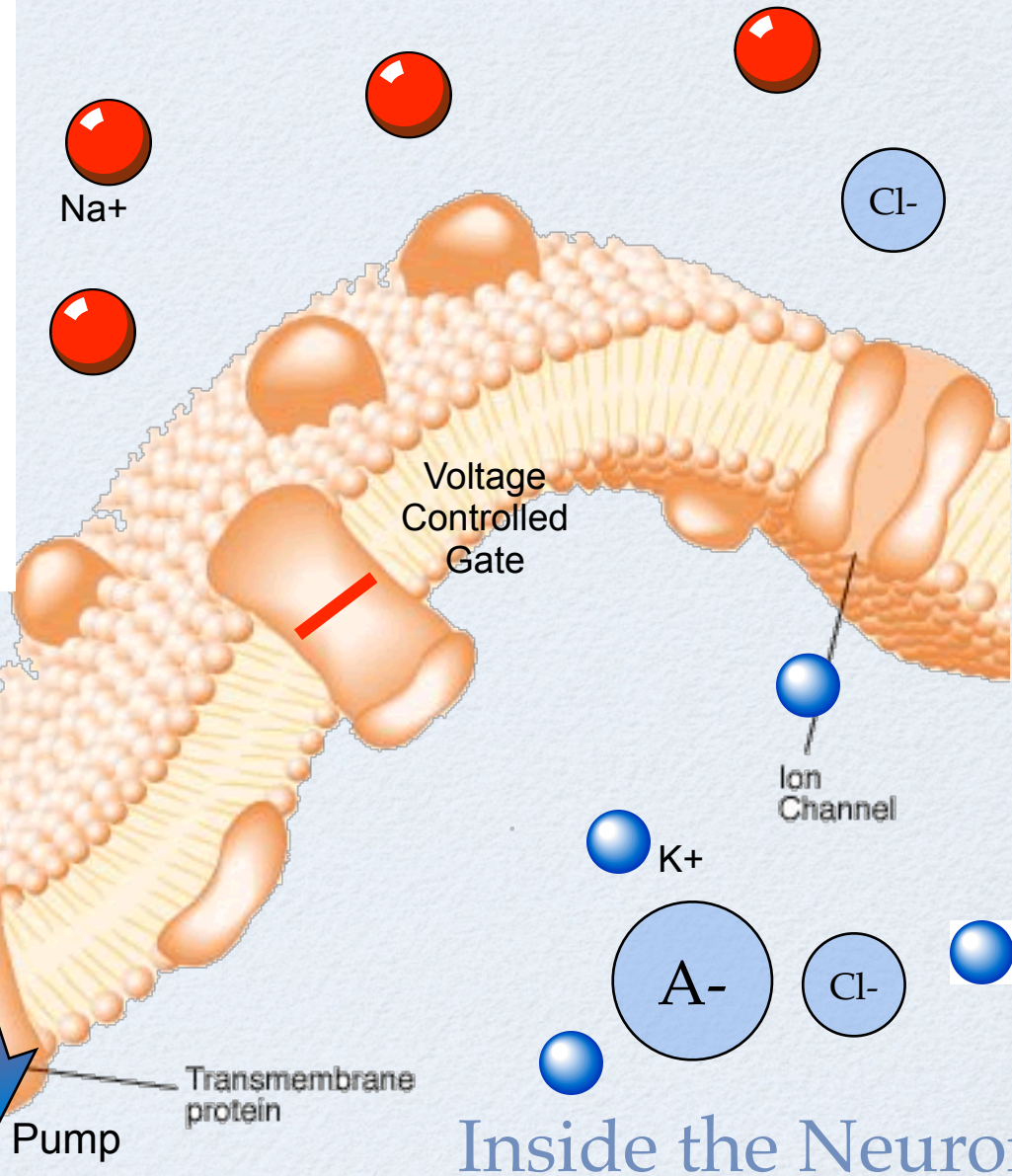
Driving force		Net driving force \times Permeability (P)	Net flux
Chem.	Elec.		
Extracellular side Na^+	+++	$\downarrow \times P_{\text{Na}} = \downarrow$	\downarrow
Cytoplasmic side Na^+	---		
Extracellular side K^+	+++	$\uparrow \times P_{\text{K}} = \uparrow$	\uparrow
Cytoplasmic side K^+	---		
Extracellular side Cl^-	+++	$\longleftrightarrow \times P_{\text{Cl}} = \longleftrightarrow$	\longleftrightarrow
Cytoplasmic side Cl^-	---		



Net Force at Rest

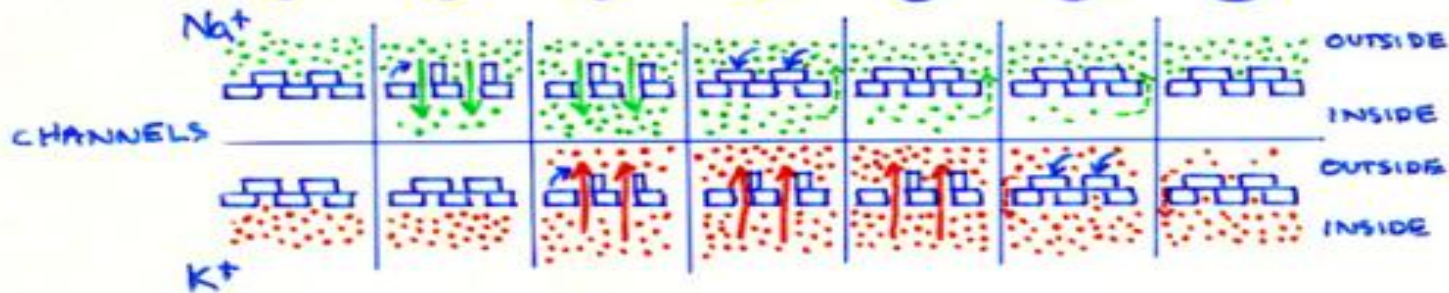
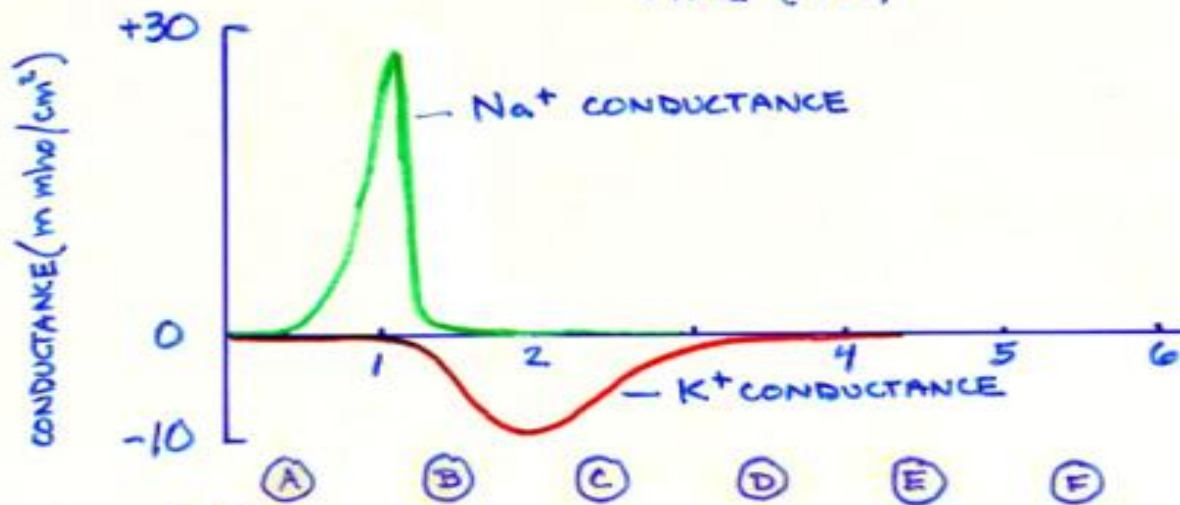
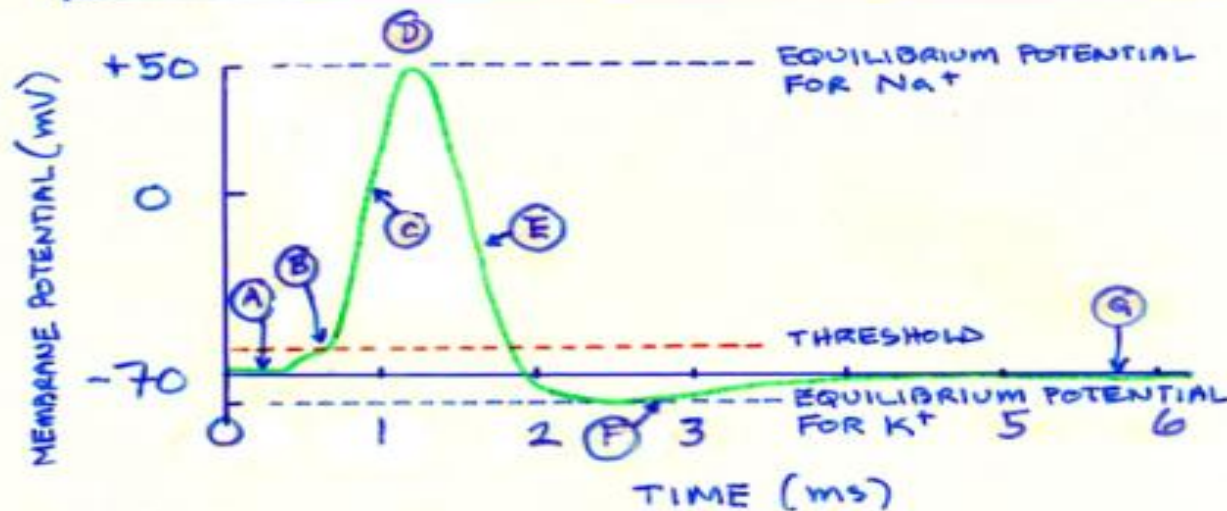
Driving force		Net driving force x Permeability (P_i)	Net flux
Chem.	Elec.		
Extracellular side	Na^+	+++	↓ $\times P_{\text{Na}} =$ ↓
Cytoplasmic side	Na^+	---	
Extracellular side	K^+	+++	↑ $\times P_{\text{K}} =$ ↑
Cytoplasmic side	K^+	---	
Extracellular side	Cl^-	+++	↔ $\times P_{\text{Cl}} =$ ↔
Cytoplasmic side	Cl^-	---	

Outside the Neuron



Inside the Neuron

THE ACTION POTENTIAL : VOLTAGE & CONDUCTANCE

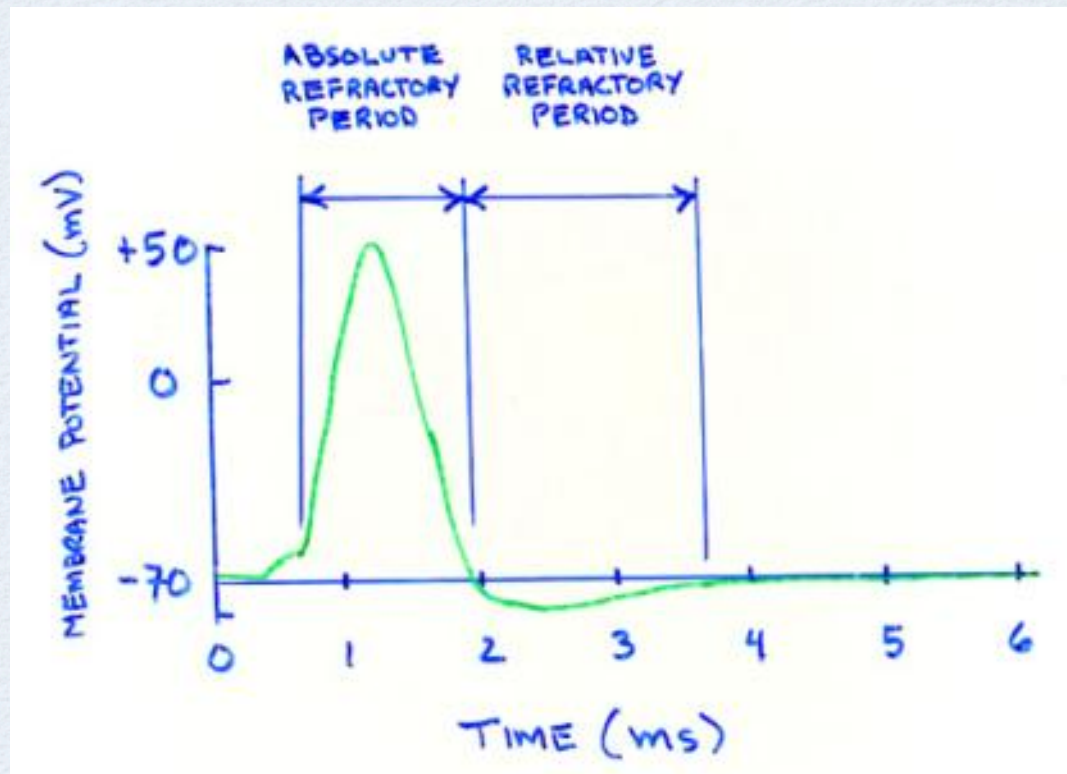


- B: Na open
- C: K open
- D: Na close
- E: Na pump
- F: K close
- G: Pumps

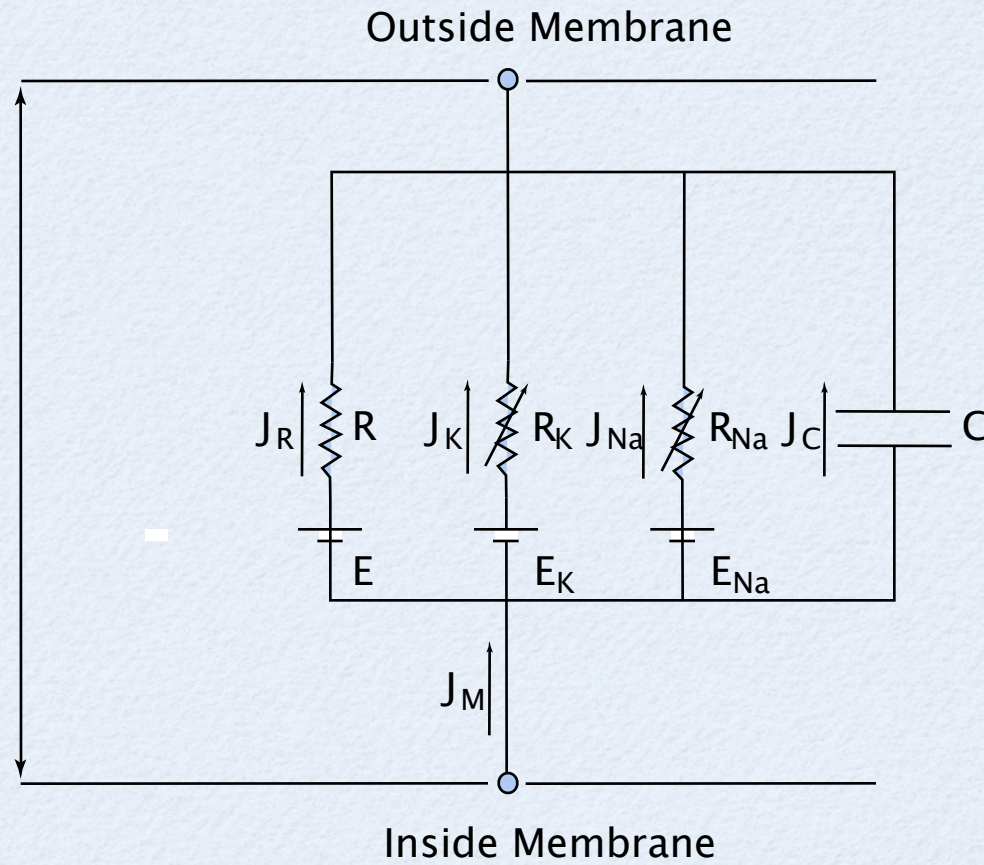
K-Na pump

→

- Absolute: Na channels are open or recovering.
No second spike
- Relative: K channels are open membrane is hyperpolarized (-80mV), so hard to generate 2nd spike (usually from -70mV)



Hodgkin-Huxley circuit



Class II circuit

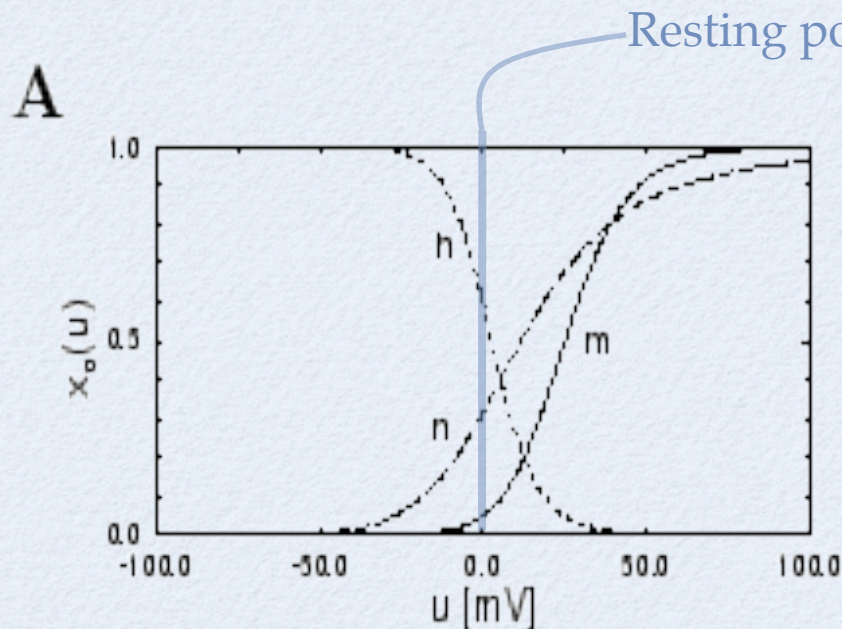
Hodgkin-Huxley equations

- 4D nonlinear differential equation

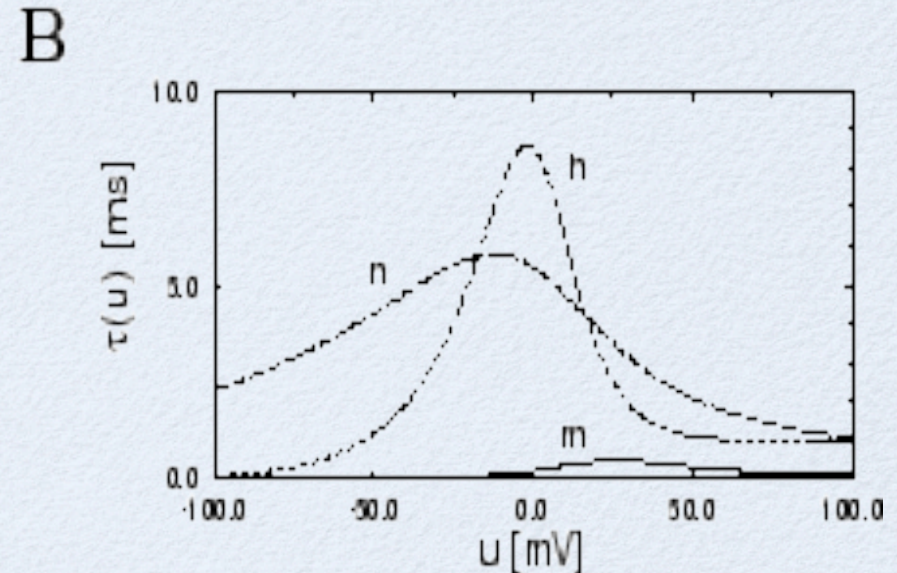
$$\begin{aligned}C \frac{dV}{dt} &= -g_{Na} m^3 h (V - E_{Na}) - g_K n^4 (V - E_K) - g(V - E) + J_M \\ \frac{dm}{dt} &= \frac{1}{\tau_m(V)} (-m + M(V)) \\ \frac{dh}{dt} &= \frac{1}{\tau_h(V)} (-h + H(V)) \\ \frac{dn}{dt} &= \frac{1}{\tau_n(V)} (-n + N(V)).\end{aligned}$$

HH parameter dynamics

- m , n activation; h , inactivation params
- all approach some asymptote (e.g., $N(V)$) with a time constant (e.g., τ_n).

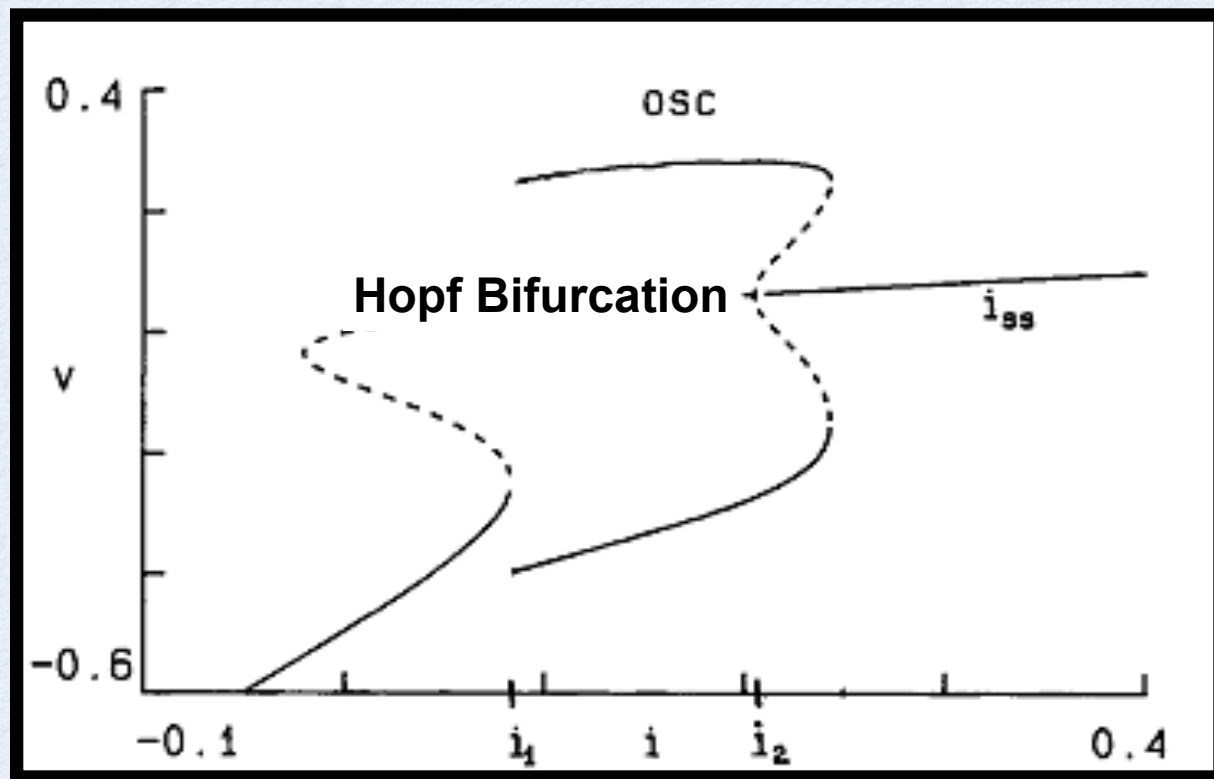


Asymptotic V value (x%)



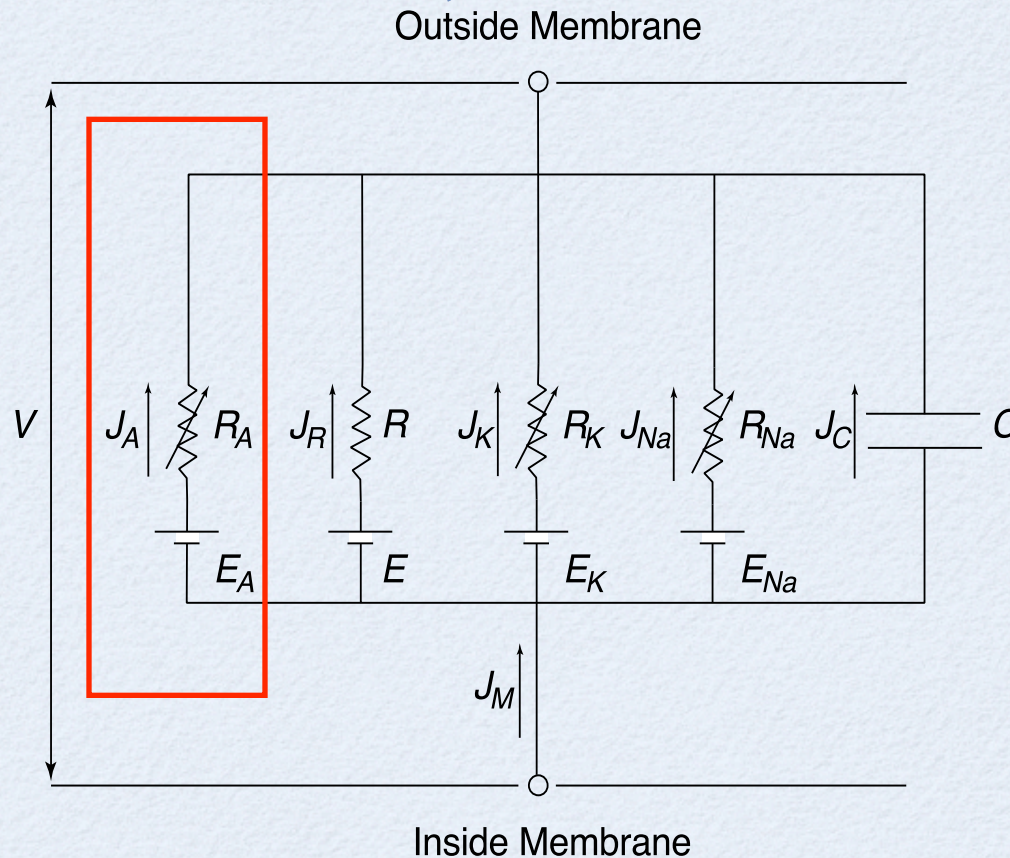
Time constant to x

HH Dynamics: Hopf



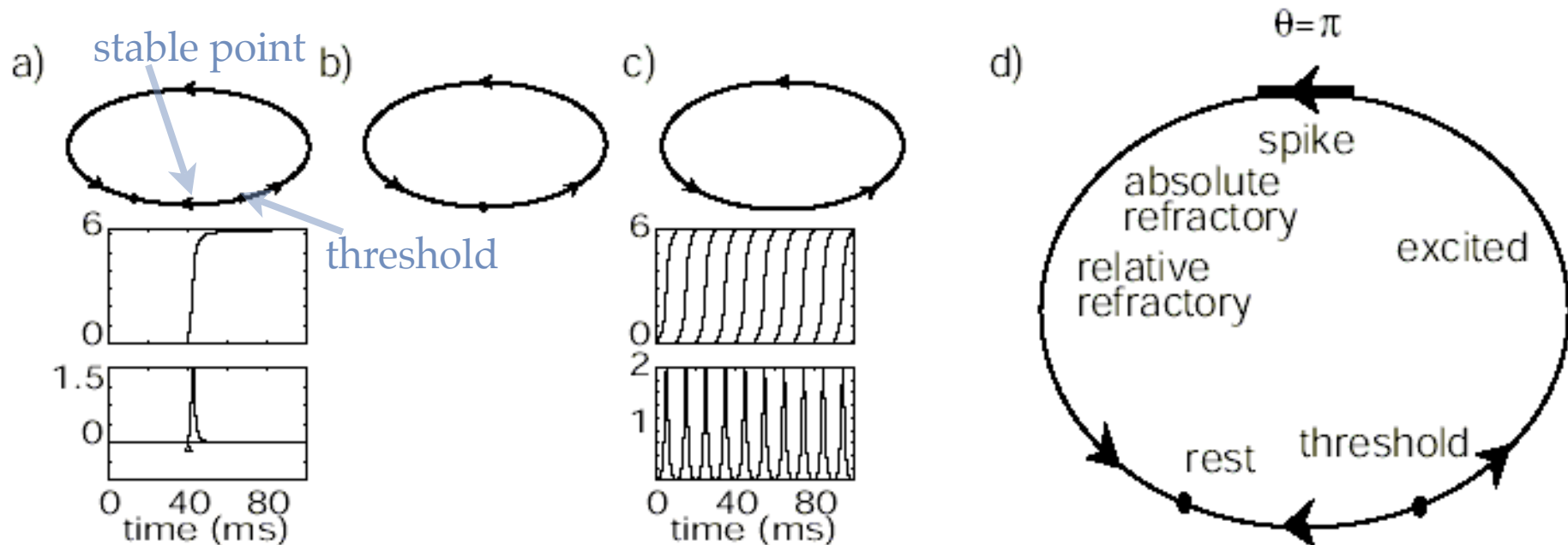
Class I circuit

- zero minimum spiking hz and grow monotonically
- need to add A-current, another fast K current



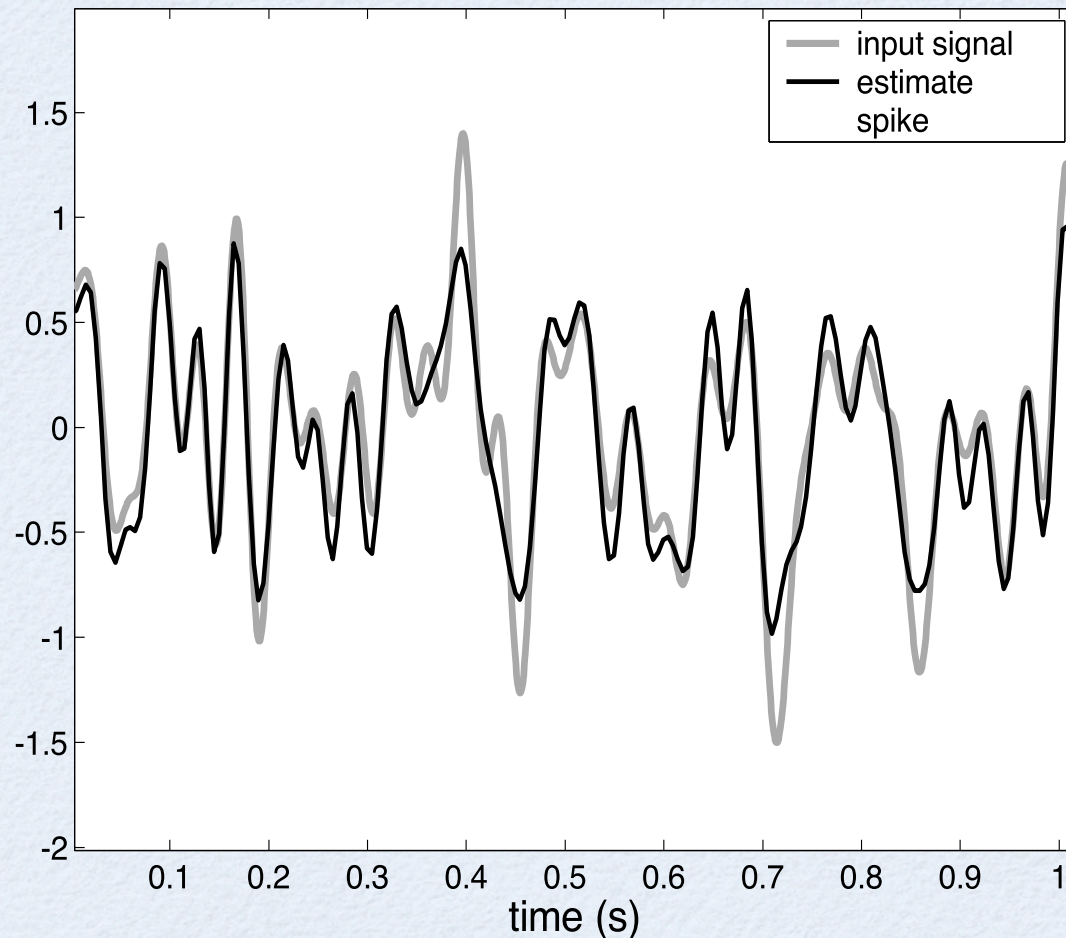
Theta neuron behaviour

- Canonical model of saddle-node bifurcation
- Phase variable maps to neural states



Theta neuron decoding

- Takes 100x longer than LIF to run



Wilson Neuron (reduced)

- Start with a HH neuron model. Rinzel simps:
 - Na activation is very fast ($\tau(V)$ is really small), so allow $m=M(V)$ (no dynamics)
 - Na inactivation is equal and opposite to K activation, so let $h=1-n$ (combine h & $n \rightarrow R$)
- We need the A-current. Rose & Hindmarsh simp:
 - Make the dynamics for R quadratic.
- Include adaptation variable with slow dynamics
- Have 3D class I model!

Wilson neuron equations

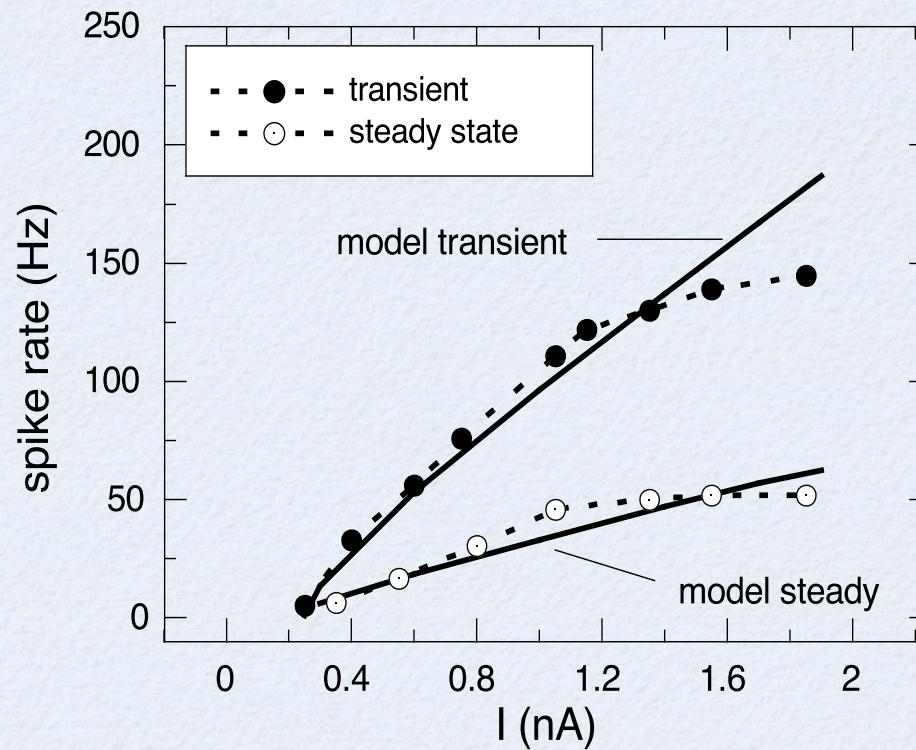
$$C \frac{dV}{dt} = - (1781 + 4758V + 3380V^2) (V - 48)$$

$$- 26R(V + 95) - 13H(V + 95) + J_M$$

$$\frac{dR}{dt} = \frac{1}{5.6} (-R + 129V + 79 + 330(V + 38)^2)$$

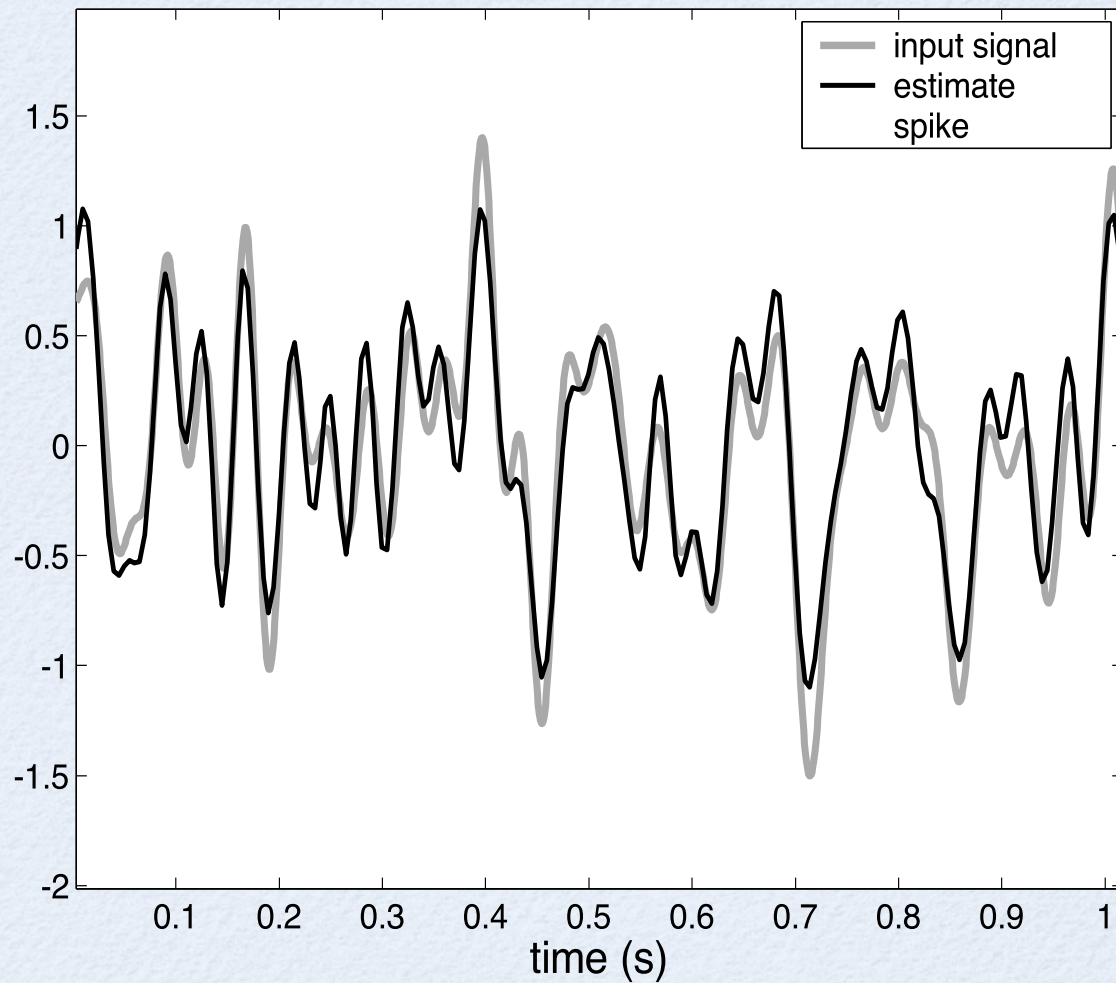
$$\frac{dH}{dt} = \frac{1}{99.0} (-H + 11(V + 75.4)(V + 69)).$$

- Comparison of Wilson neuron and real data



- Pros: it's a class I, adapting neuron with spike dynamics; captures spike height changes, spike shape, and after-hyperpolarizations (overshoot of the resting value after a spike)
- Cons: 600x slower than LIF

Wilson neuron decoding



Comparison of neurons

Neuron	Rate	Bits/spike	RMSE	Run time (s)
LIF	114	1.24	0.153	0.18
Adapting LIF	114	2.23	0.153	0.24
θ -Neuron	109	0.96	0.160	20.1
Wilson Model	91	2.00	0.186	125.2

Summary

- variety: 'phenomenological' models through to more complete models that include adaptation, spike dynamics, and ion channel dynamics.
- We haven't discussed are compartmental models.
(<http://diwww.epfl.ch/~gerstner/SPNM/node17.html>).
- All of the models have info rates between 1-3 b/s
- Adaptation seems to help improve efficiency
(using Gaussian white noise here)
- LIF are very computationally efficient and have reasonable info trans efficiency.